

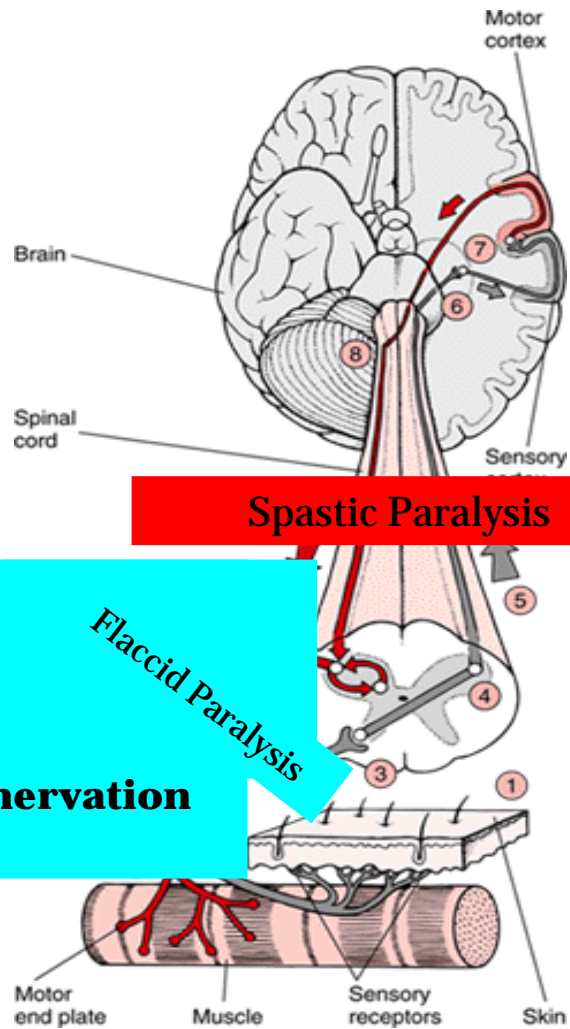
Simulating Hodgkin-Huxley-like Excitation using Comsol Multiphysics

Martinek^{1,2}, Stickler², Reichel¹ and Rattay²

¹ Department of Biomedical Engineering and Environmental Management, University of Applied
Sciences Technikum Wien, Vienna, Austria

² Institute for Analysis and Scientific Computing, Vienna University of Technology, Austria

Goal of Simulation - Clinical View

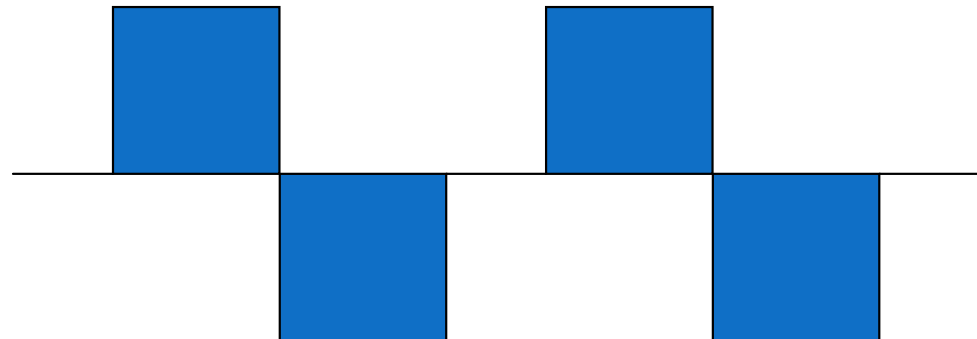
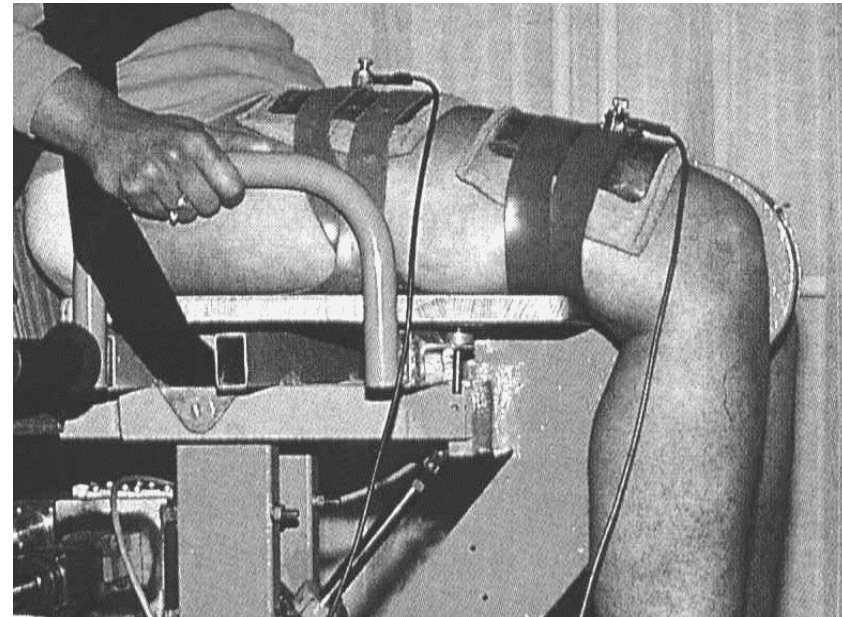


Spastic Paralysis

Flaccid Paralysis

Denervation

Large Surface Electrodes



Long Impulses

Goal of Simulation - Modeling View

- Model of Single Fiber
 - **Hodgkin-Huxley**
- Electrical Field Distribution
- Coupling
 - Reaction of fiber in external Electrical Field

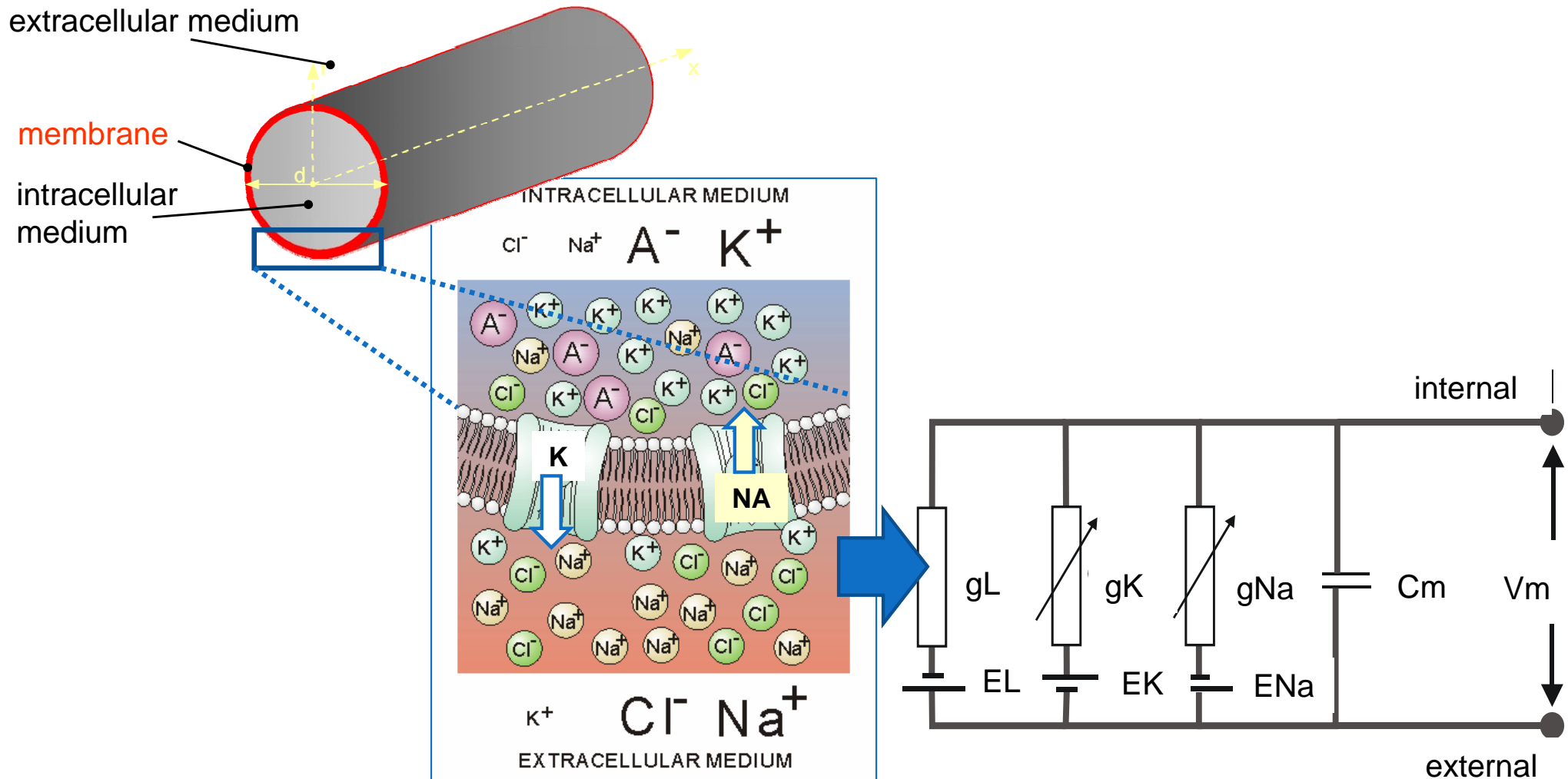
History of Hodgkin-Huxley Model

- Hodgkin and Huxley experimented on squid giant axon and explored how the Action Potential is produced in the (nerve) fiber (Journal of Physiology, 1952)

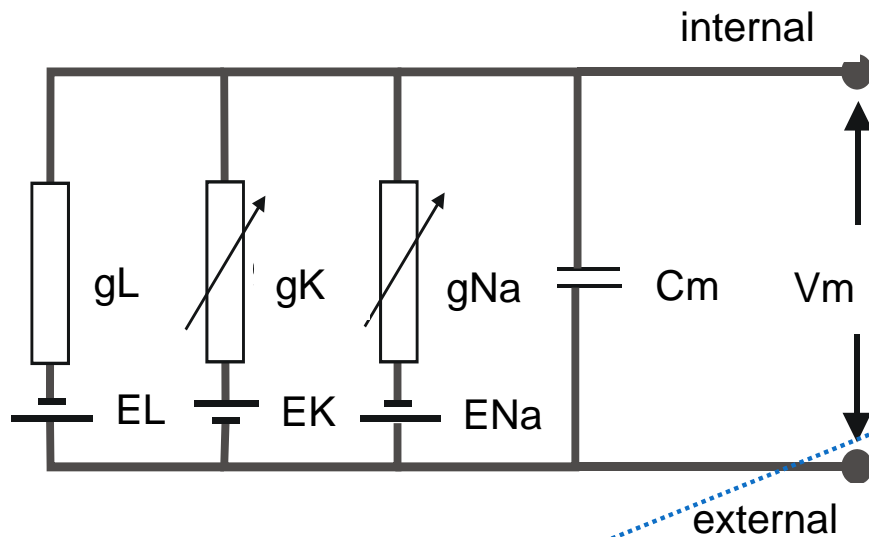


- Hodgkin and Huxley awarded the 1963 Nobel Prize for the model

The muscle fiber - membrane



Hodgkin-Huxley PDE



$$C_m \frac{dV}{dt} = I_{ext} + I_{NA} + I_K + I_L$$

C_m ... capacitance of membrane

r ... radius of axon

ρ ... resistance of intracellular space

g_{Na}, g_K, g_L, \dots conductance of Natrium, Potassium and Leakage

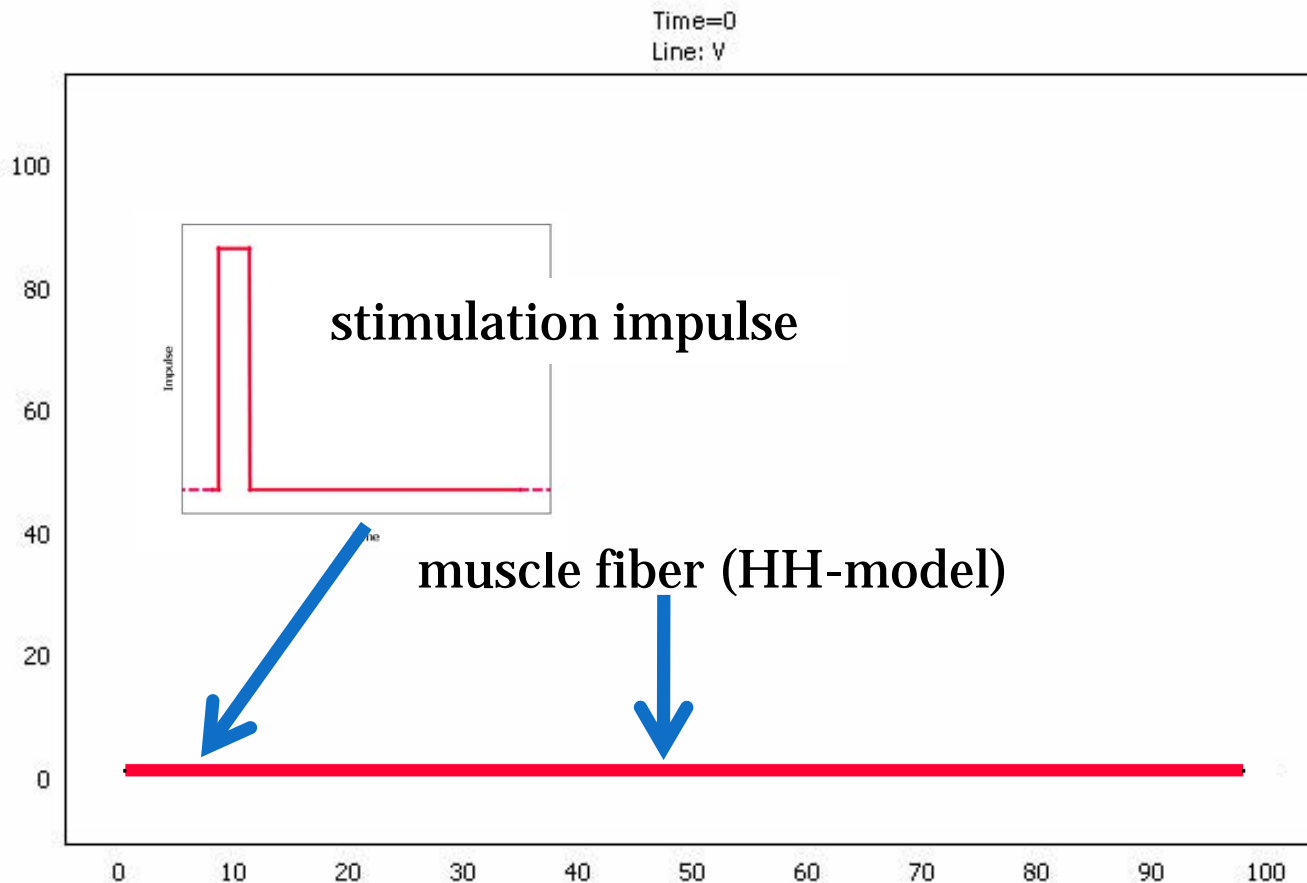
$$C_m \frac{dV}{dt} = \frac{r}{2\rho} \frac{\partial^2 V}{\partial x^2} - g_{Na} m^3 h (V - V_{Na}) - g_K n^4 (V - V_K) - g_L (V - V_L)$$

$$\frac{dw}{dt} = \alpha_w (1 - w) - \beta_w w \quad (w \text{ is } m, n \text{ or } h)$$



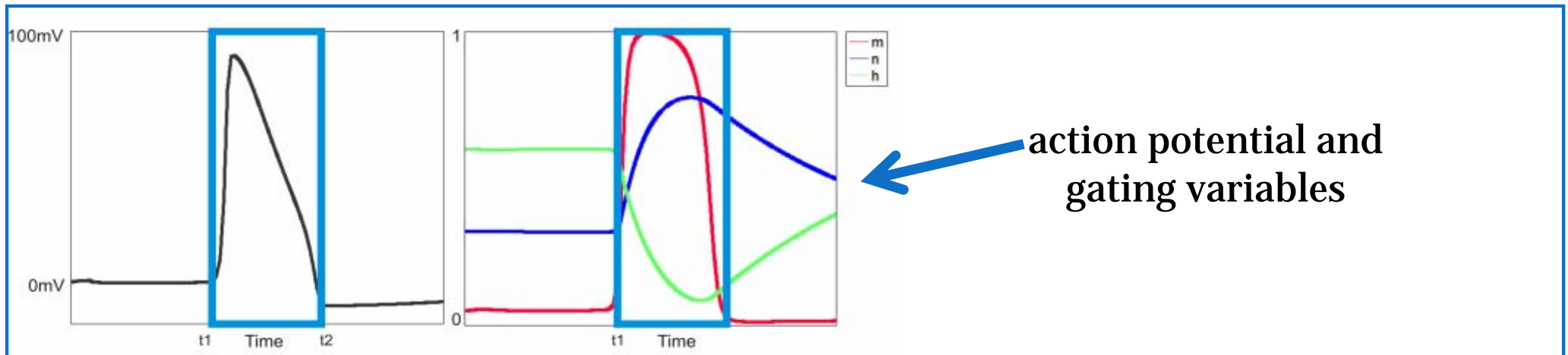
System of
1 non-linear and
3 linear differential equations

1D muscle fiber model

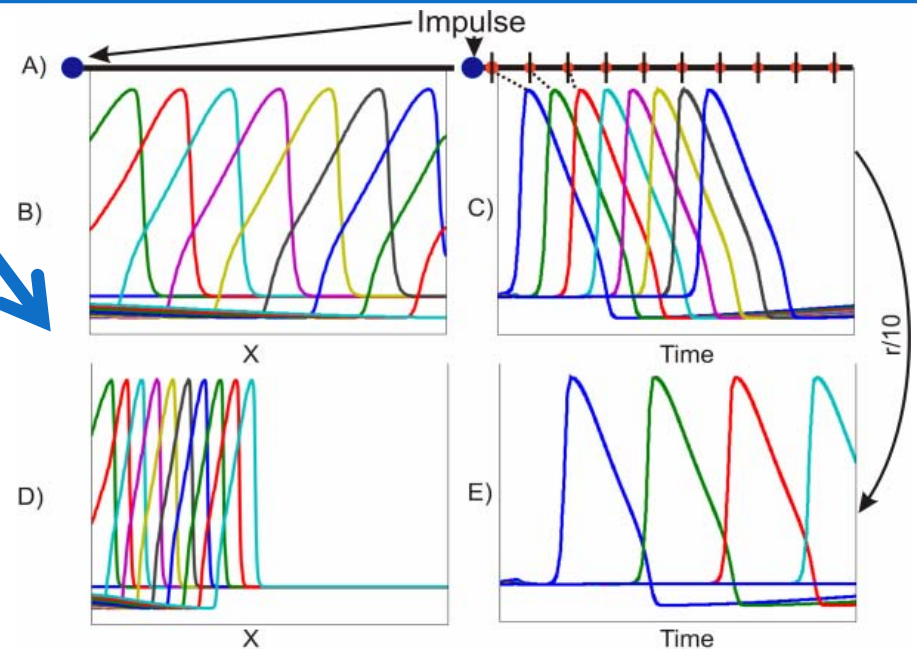


App. Mode	PDE – Coeff. Form
Dimension	1D
Dep. Variables	4: V, m, n, h
N. of Elements	200
Solver	Direct (UMFPACK) Time dependent (0:0.1:10)
rel. Tolerance	10e-5
abs. Tolerance	10e-7
Solution Time	<30 sec

1D muscle fiber

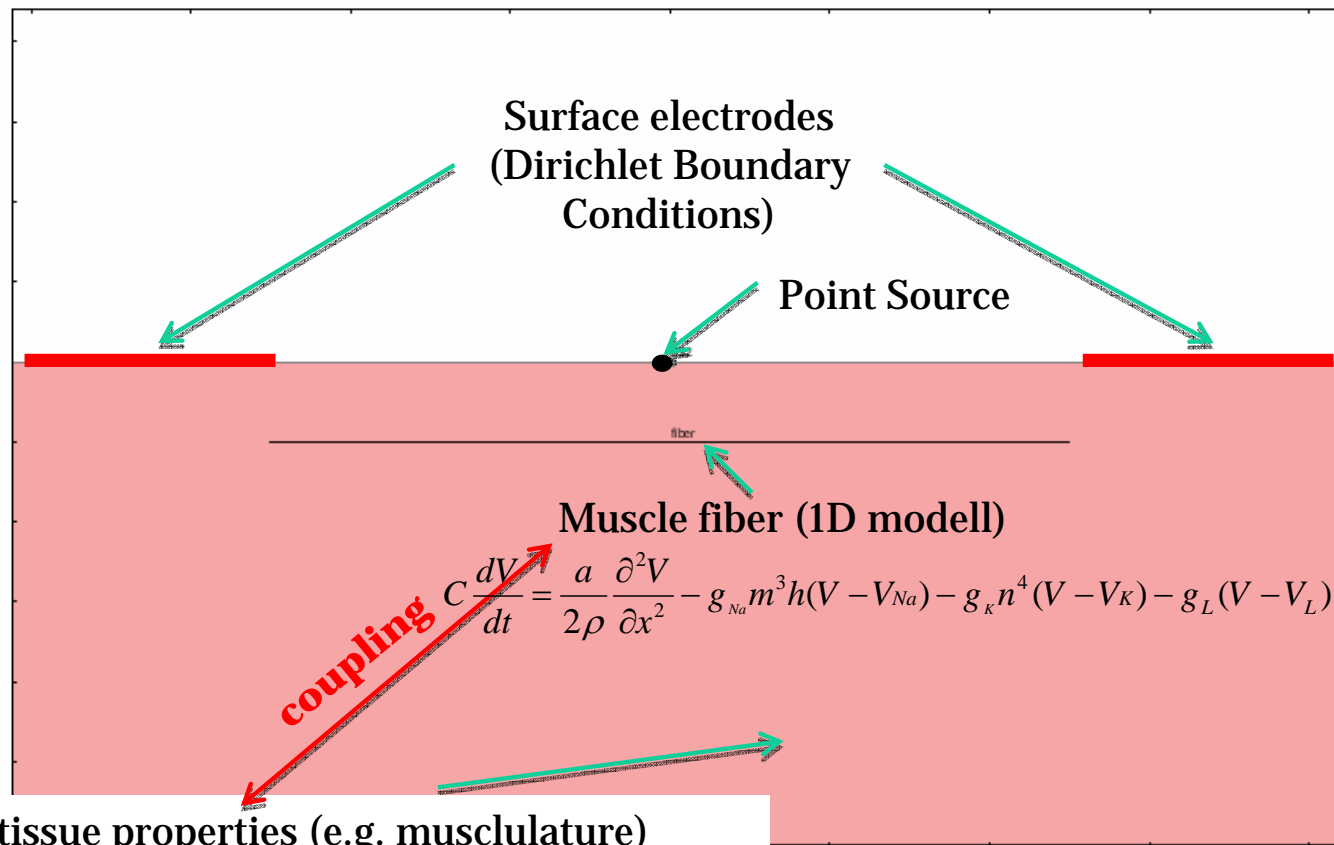


change of radius



Results are comparable to e.g. „Hodgkin AL, Huxley AF, **A quantitative description of membrane current and its application to conduction and excitation in nerve**, J Physiol, **117**, 500-544 (1952)”

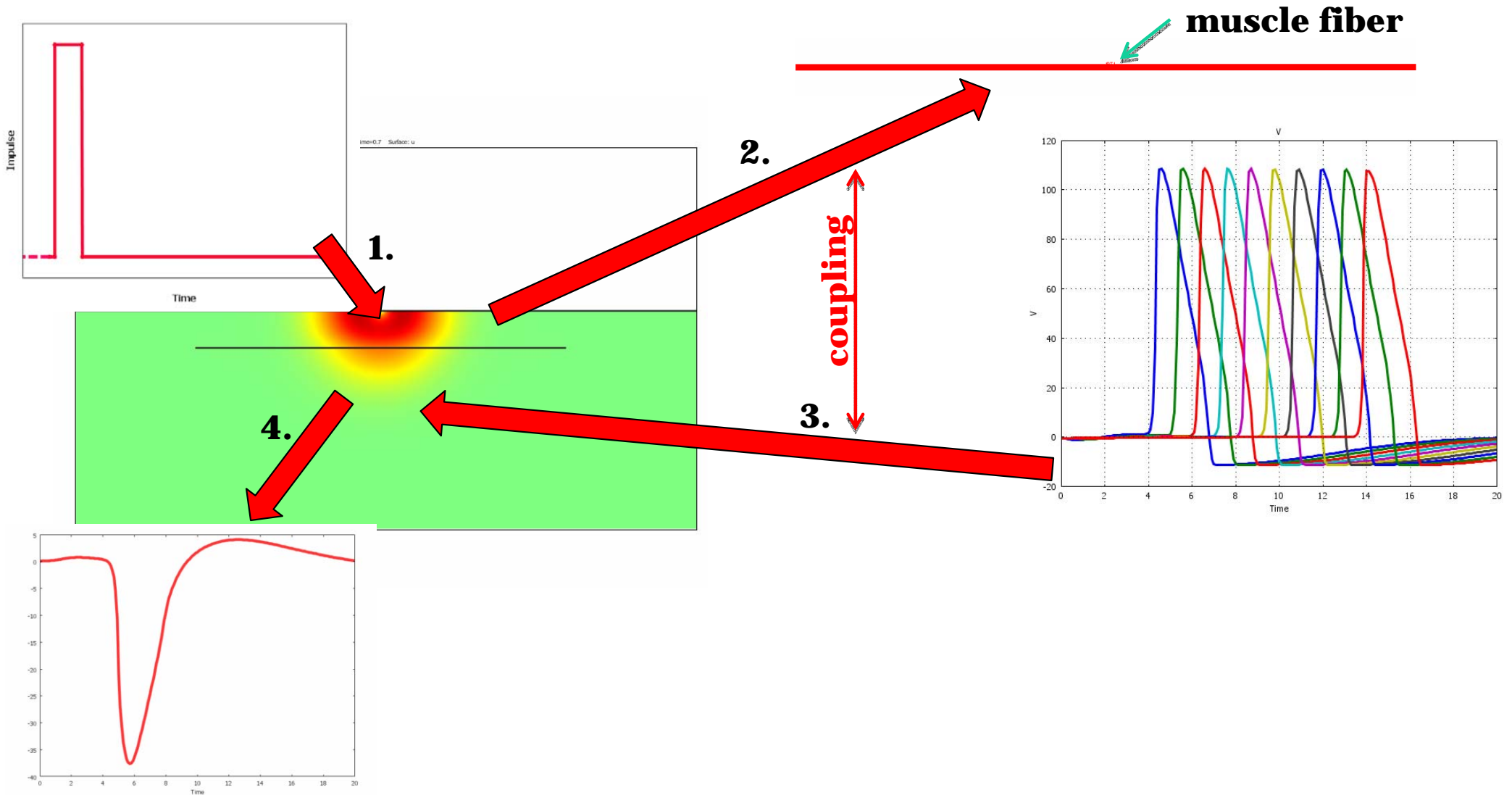
2D model



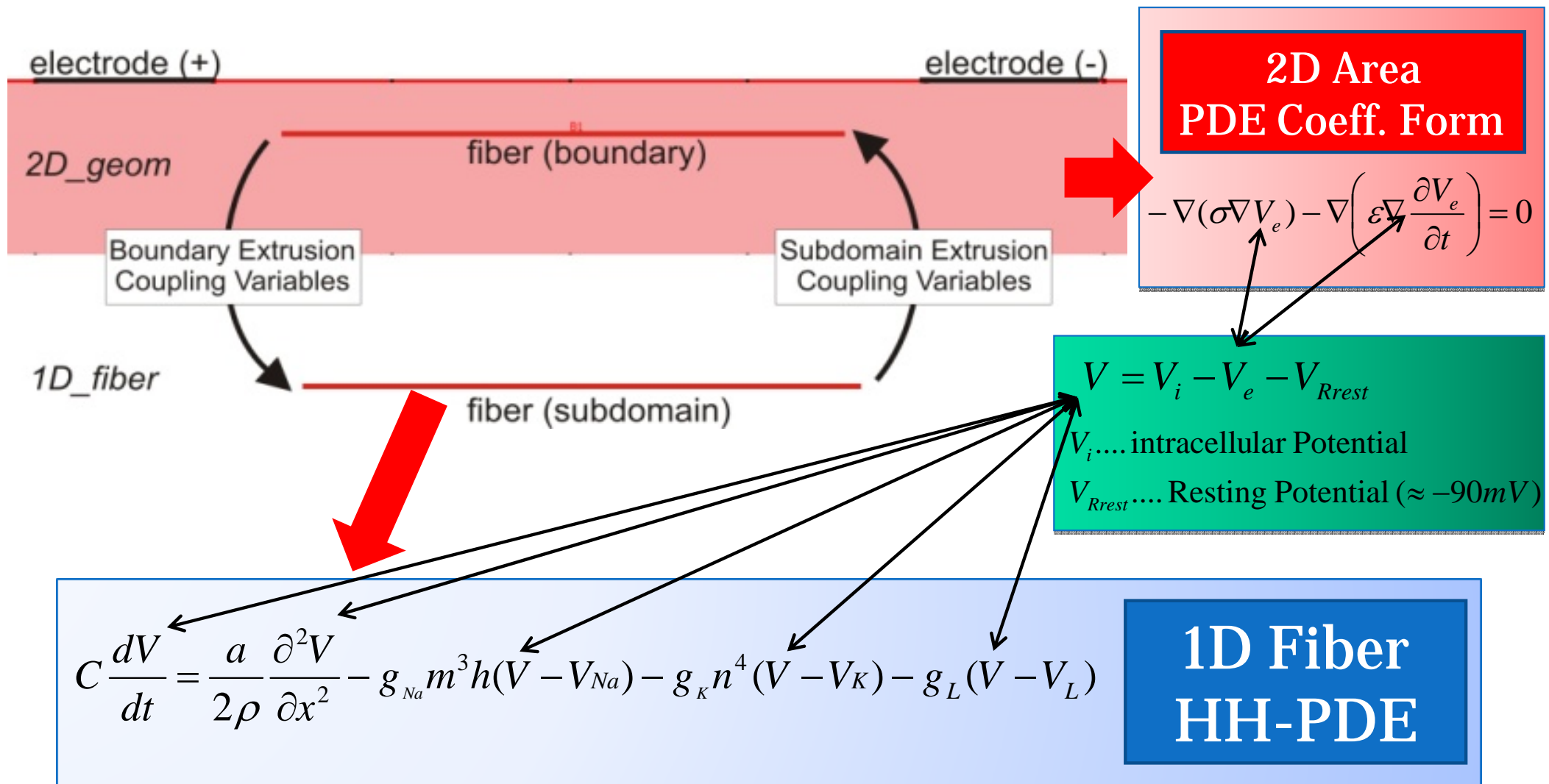
$$-\nabla(\sigma \nabla V_e) - \nabla \left(\varepsilon \nabla \frac{\partial V_e}{\partial t} \right) = 0$$

App. Mode	PDE – Coeff. Form
Dimension	2D & 1D
Dep. Variables	4 (1D): V_i, m, n, h 1 (2D): V_e
N. of Elements	1D: 200 2D: ca. 12000
Solver	Direct (UMFPACK) Time dependent (0:0.1:10)
rel. Tolerance	10e-5
abs. Tolerance	10e-7
Solution Time	<600 sec

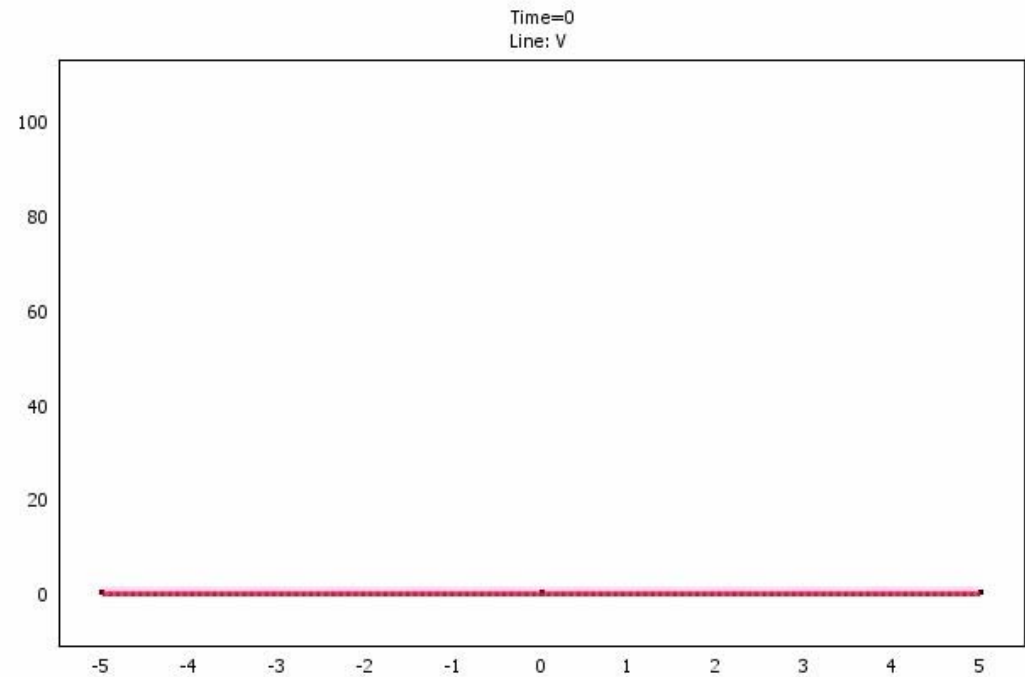
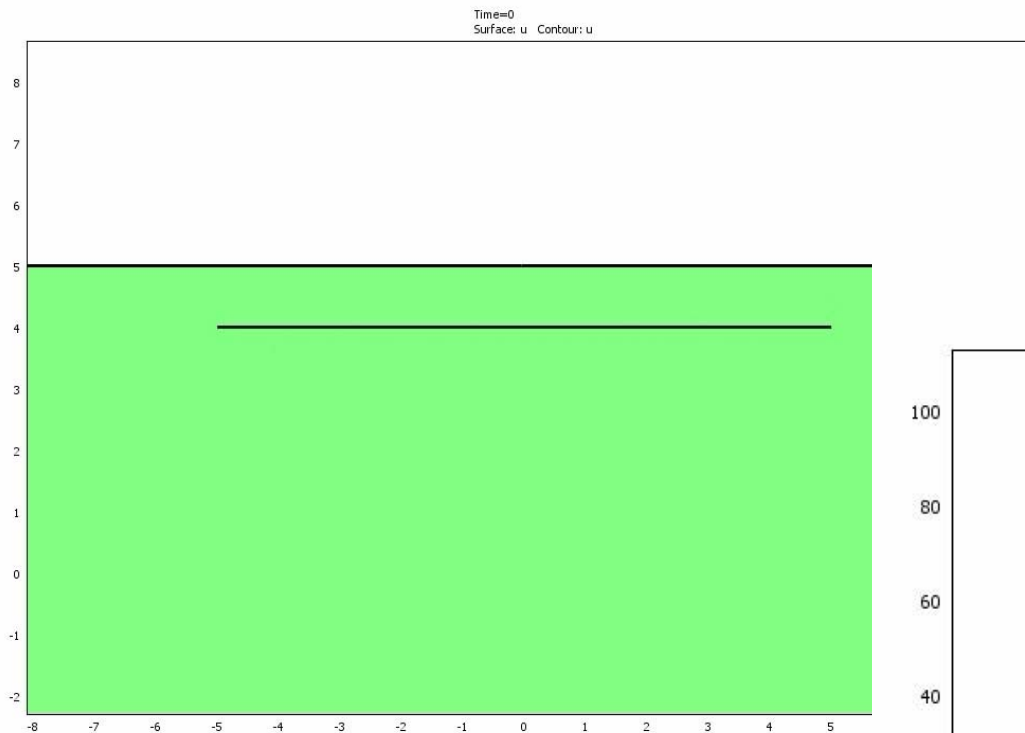
2D model - Coupling („real life“)



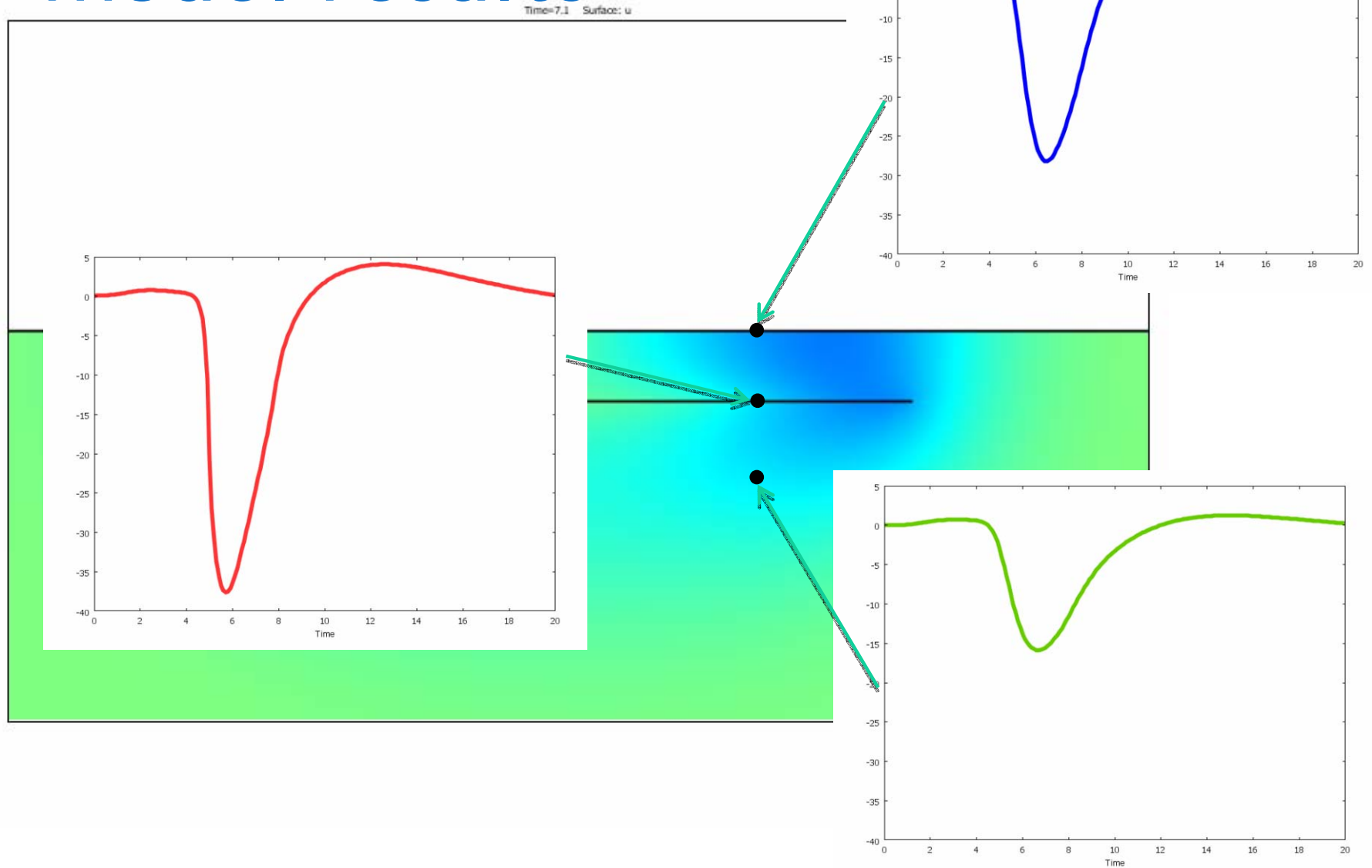
2D model - Coupling („model“)



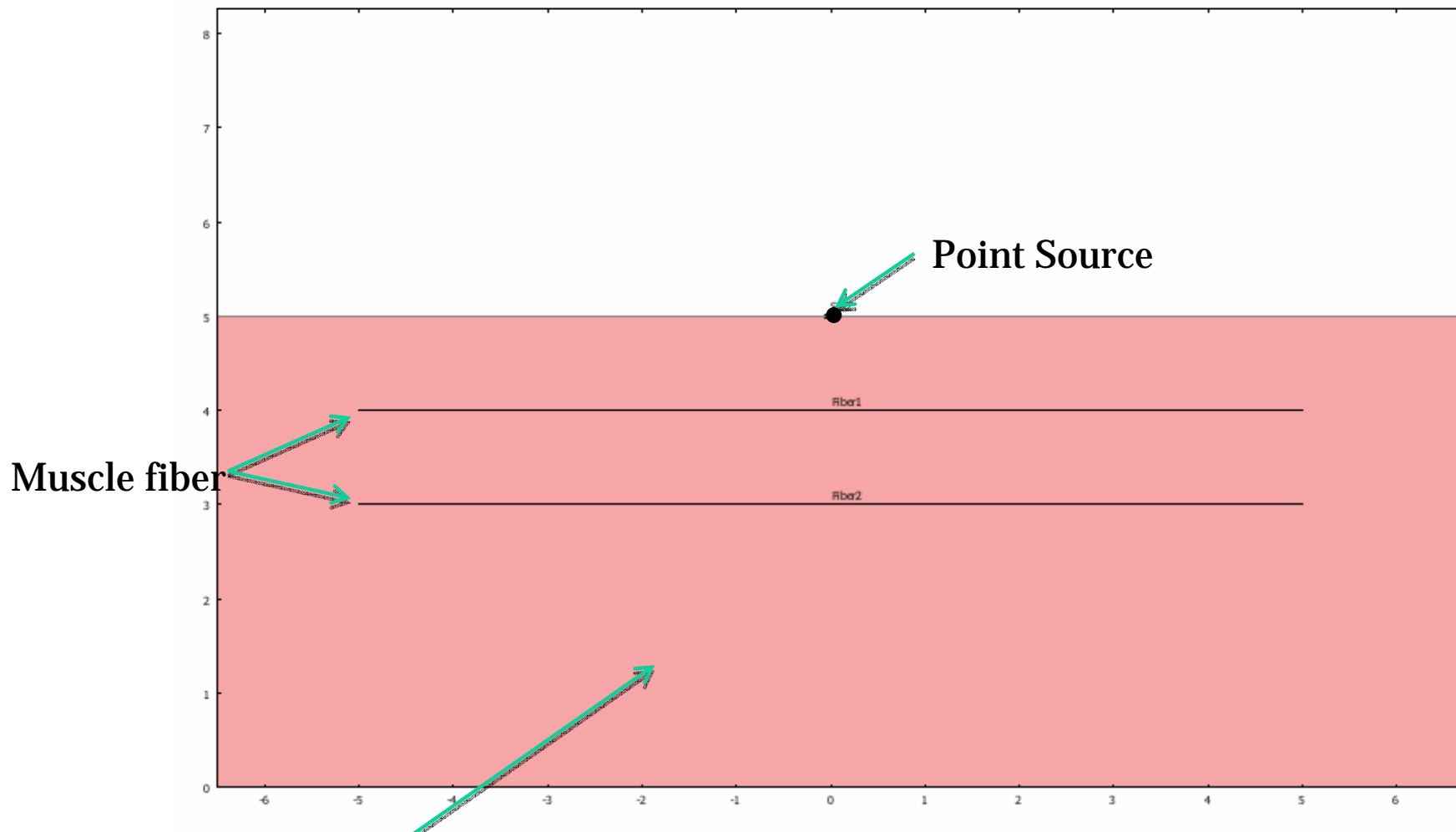
2D model - Animation



2D model results

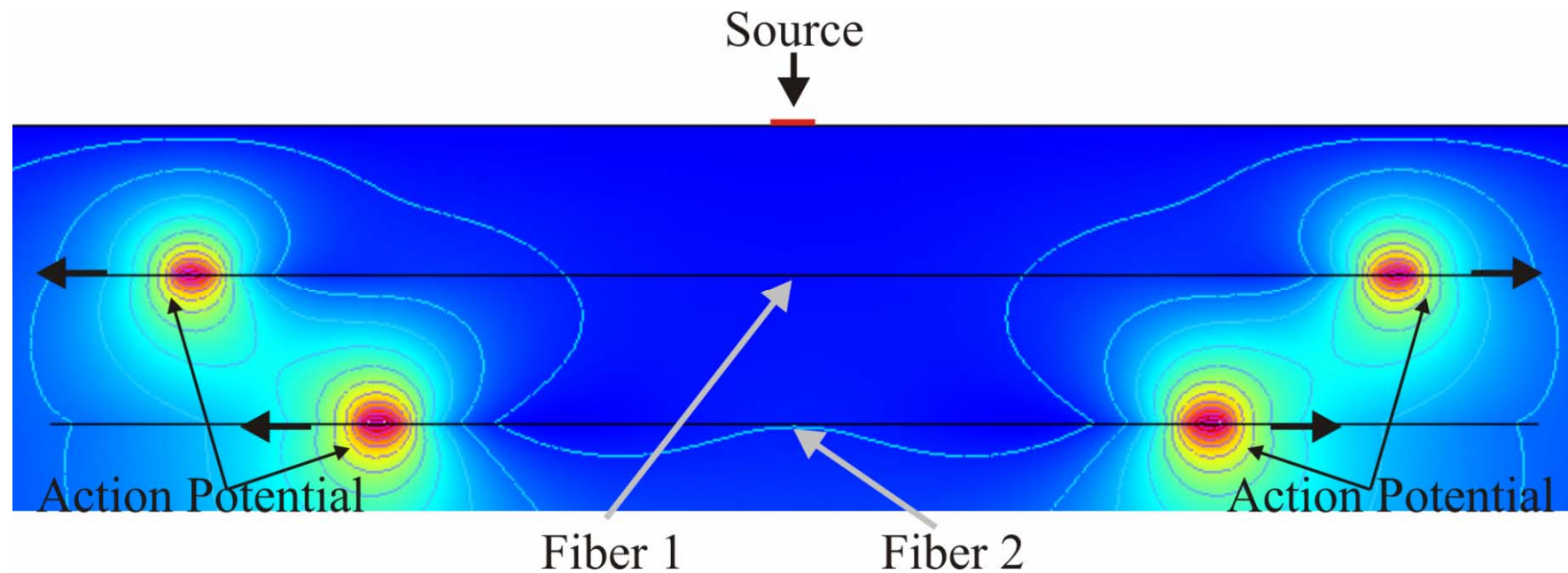


2D model - 2 fibers

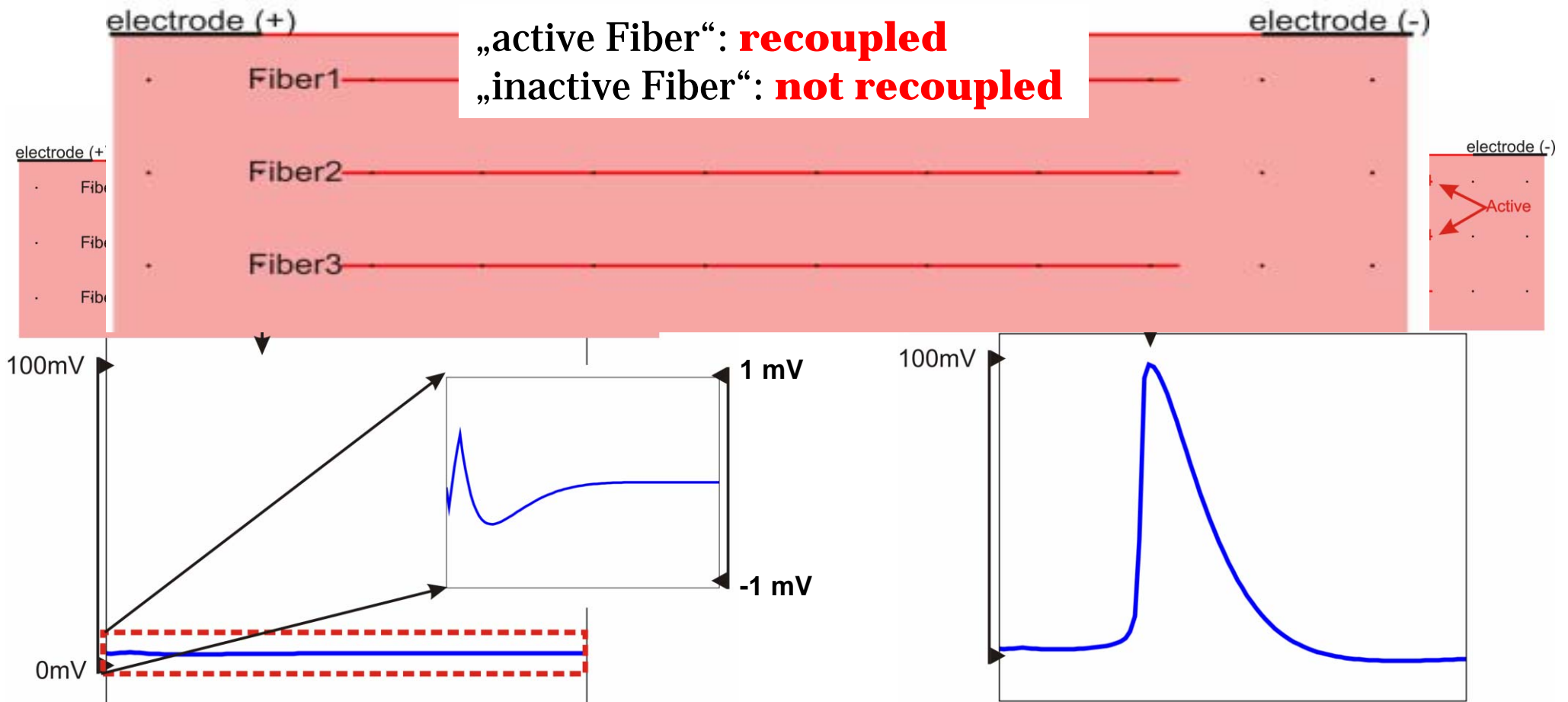


tissue properties (e.g. musculature)

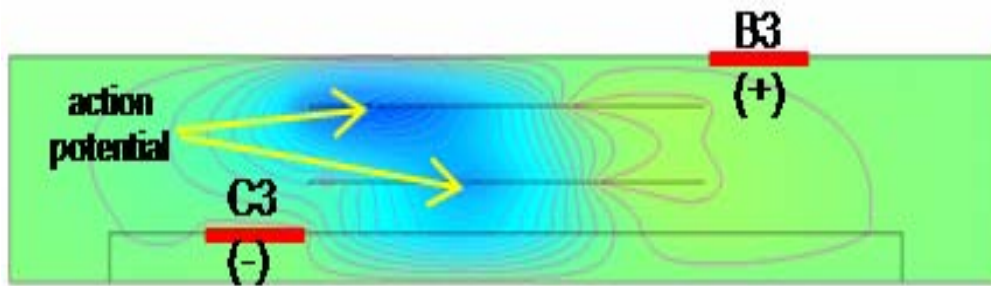
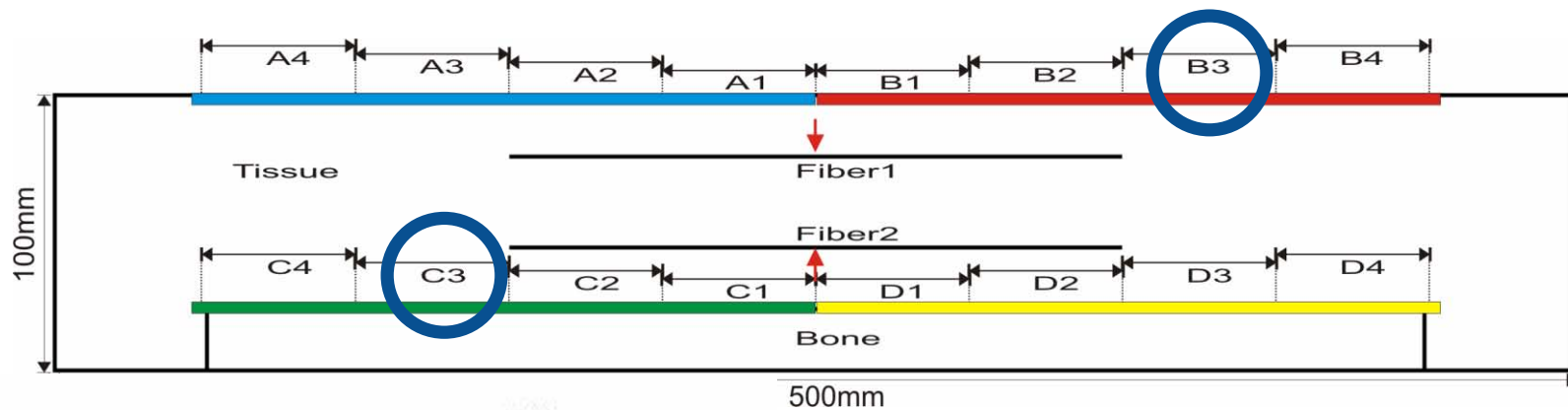
2D model - 2 fibers



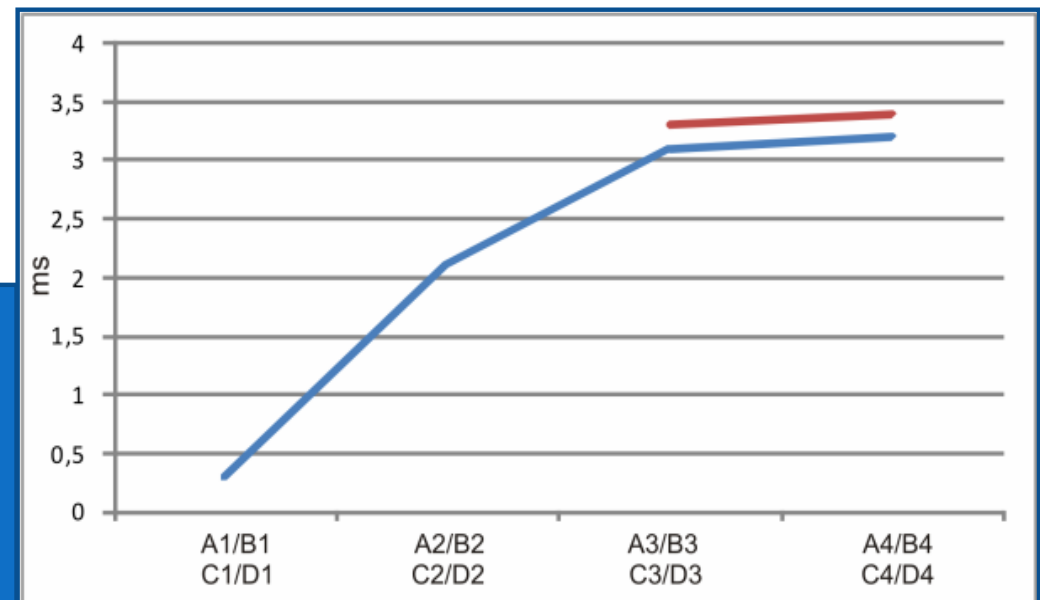
2D model - Influence of fibers



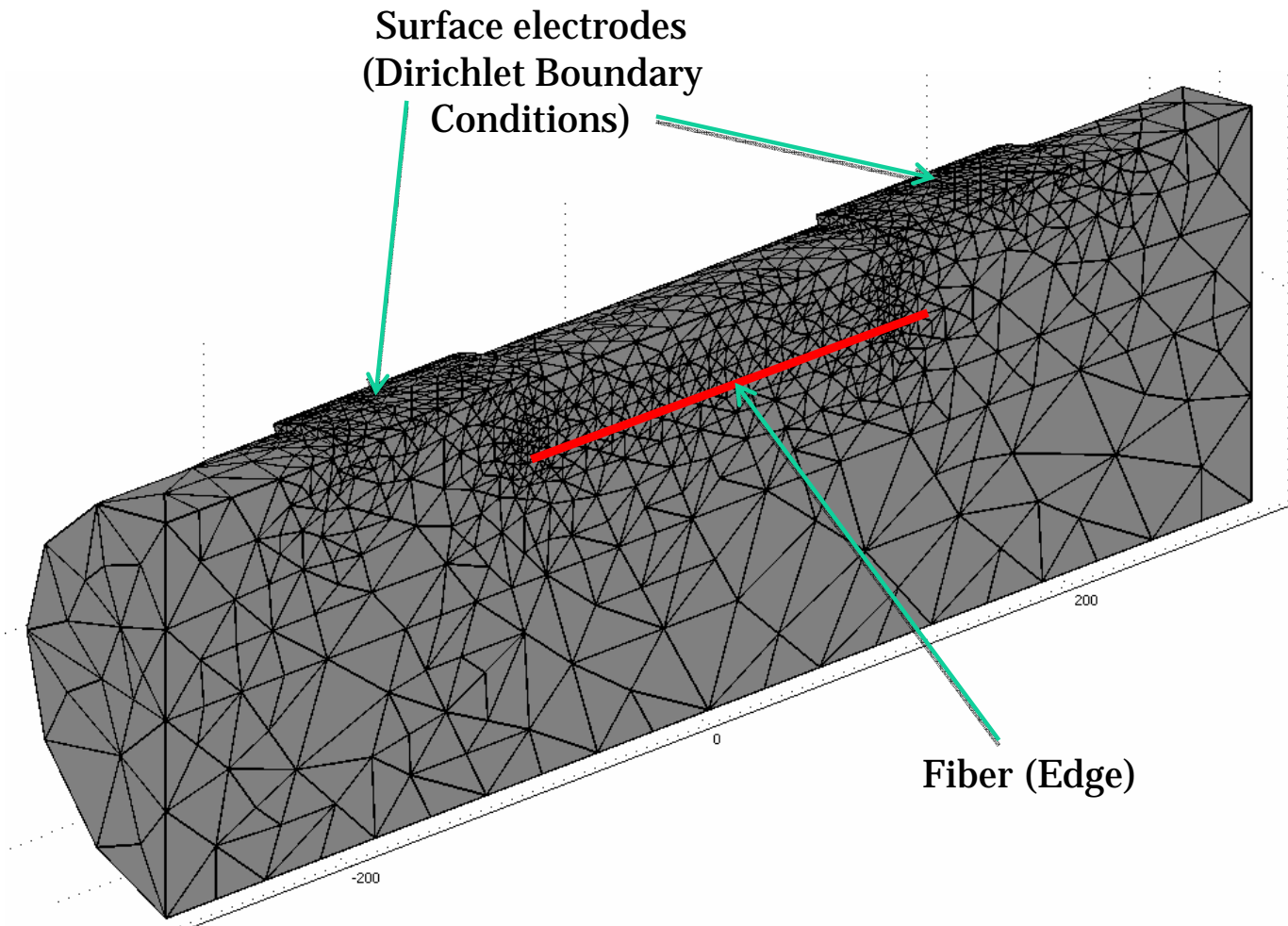
Influence of electrodes position



Time from stimulation impulse till an action potential is initiated. The diagram shows the excitation time of different electrode positions at the surface and implanted electrodes. The red line represents the fiber placed closer to the electrodes. The blue line is representing the more distant fiber.



Outlook - 3D model



App. Mode	PDE – Coeff. Form
Dimension	3D & 1D
Dep. Variables	4 (1D): V_i, m, n, h 1 (3D): V_e
N. of Elements	1D: 200 3D: ca. 30000
Solver	Different solvers Time dependent (0:0.1:10)
rel. Tolerance	$10e-5$
abs. Tolerance	$10e-7$
Solution Time	Very long ☹

Future Work

- Adaption of model parameters (denervated muscle,)
- Implementation of musclepaths ?
- Creation of 3D geometry (CT / MRI based ?)
-

Conclusion / Discussion

- **HH PDE & Comsol Multiphysics are a great combination to**
 - Easily create models with different geometries
 - Coupling of extracellular and intracellular potential in **both** directions
 - Simulation of effects of stimulation and generated action potentials

Questions ?!?

Thank you for your
attention !!!