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Parameter Optimization for FEM based modeling of singlet oxygen during PDT using COMSOL

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- Introduction
- Theory for PDT dosimetry model
- Optimization results
- PDT dosimetry quantity prediction for prostate using COMSOL
- Conclusions

#### Introduction

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# Introduction

- Photodynamic therapy (PDT) is an important treatment modality for cancer and other localized diseases.
- In PDT, photosensitizers excited by light react with ground state oxygen, which leads to generation of singlet oxygen the major cytotoxic agent - to kill the surrounding tissues and cells.
- Compared with other treatment modalities, PDT has advantages including non-ionizing, localized photon delivery and better cosmetic outcome.

# Introduction

#### Jablonski Diagram for Type II PDT interaction



Sensitizer (PS) + light + oxygen  $({}^{3}O_{2}) \rightarrow singlet oxygen ({}^{1}O_{2})$ 

# Introduction

Apparent reacted singlet oxygen  $[^{1}O_{2}]_{rx}$  was introduced as a PDT dosimetry quantity to better predict the PDT treatment outcome than PDT dose



By COMSOL + MATLAB

By COMSOL

Flow chart for PDT photophysiological parameter optimization and dosimetry prediction

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## Theory for PDT dosimetry model

Light diffusion equation

$$\mu_a \varphi - \nabla \cdot \left(\frac{1}{3\mu_s} \nabla \varphi\right) = S$$

 $[^{\circ}O_{2}] + \beta$ 

→ COMSOL

Photo chemical equations

$$\frac{d[S_0]}{dt} + \left(\xi \frac{\varphi([S_0] + \delta)[{}^{3}O_2]}{[{}^{3}O_2] + \beta}\right)[S_0] = 0$$

$$\frac{d[{}^{3}O_2]}{dt} + \left(\xi \frac{\varphi[S_0]}{[{}^{3}O_2] + \beta}\right)[{}^{3}O_2] - \left(g \left(1 - \frac{[{}^{3}O_2]}{[{}^{3}O_2](t=0)}\right)\right) = 0$$
MATLAB
$$\frac{d[{}^{1}O_2]_{rx}}{dt} - \left(\xi \frac{\varphi[S_0][{}^{3}O_2]}{[{}^{3}O_2]}\right) = 0$$

 $\varphi$  Light fluence rate [ $S_0$ ] Ground sensitizer concentration

dt

[ ${}^{3}O_{2}$ ] Ground triplet oxygen concentration [ ${}^{1}O_{2}$ ]<sub>rx</sub> Reacted singlet oxygen concentration

## Theory for optimization model



Fitting results [ $\xi$ ,  $\sigma$ ,  $\beta$ , g] and  $[{}^{1}O_{2}]_{rx}$ 

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Parameters	Final fit	Apr Fit	Apr and Aug Fit	Previous fit [1]	Published values
ξ (cm²/s/mW)	2.0×10 <sup>-3</sup>	5.0×10 <sup>-3</sup>	3.9×10 <sup>-3</sup>	2.1×10 <sup>-3</sup>	3.7×10 <sup>-3</sup> [2]
σ (1/μM)	<b>11.2</b> ×10 <sup>-5</sup>	6.6×10 <sup>-5</sup>	11.5×10 <sup>-5</sup>	7.6×10 <sup>-3</sup>	7.6×10 <sup>-3</sup> [2]
<b>β</b> (μM)	11.9	11.9	11.9	11.9	11.9 [3]
<i>g</i> (μM/s)	0.8	0.62	0.56	0.69	_
$I^{1}O_{2}J_{rx,sh}$ (mM)	0.41	0.46	0.41	0.74	_

[1] Wang et al., J. Biophoton, 2010.

[2] Mitra et al., Photochem. Photobiol, 2005.

[3] Georgakoudi et al., Photochem. Photobiol. 1997.

#### Final fitting results including experimental data from All data



Fitting results: apparent reacted singlet oxygen concentration All data April data April and August data



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# <sup>[1</sup>O<sub>2</sub>]<sub>rx</sub> prediction using COMSOL

#### Prostate geometry for prediction model







# <sup>[1</sup>O<sub>2</sub>]<sub>rx</sub> prediction using COMSOL

# PDT dosimetry quantities for treatment up to 300 s in a homogeneous prostate



Slide view of [<sup>1</sup>O<sub>2</sub>]<sub>rx</sub>

Isosurface of  $[^{1}O_{2}]_{rx}$  at 0.41 mM

Isosurface of light flucence

# $[^{1}O_{2}]_{rx,sh}$ prediction using COMSOL



#### **30 J/cm<sup>2</sup>**

75 J/cm<sup>2</sup>

150 J/cm<sup>2</sup>

# Conclusions

- PDT model including light diffusion and PDT kinetics equations
- Optimized photo-chemical parameters in the PDT model
- PDT prostate model with homogeneous properties
- Prediction of PDT dosimetry quantities for treatment

Thank you!